

1 **Feasibility Study of an Optical Caustic Plasmonic Light Scattering Sensor for Human Serum**
2 **Anti-Dengue Protein E Antibody Detection**

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19

20 **Abstract**

21 Antibody detection and accurate diagnosis of tropical diseases is essential to help prevent the
22 spread of disease. However, most detection methods lack cost-effectiveness and field-portability,
23 which are essential features for achieving diagnosis in a timely manner in developing countries.

24 To address this problem, transparent 3D printed sample chambers with a total volume of 700
25 microliters and an oblate spheroid shape were fabricated to measure green light scattering of gold
26 nanoparticles using an optical caustic focus to detect antibodies. Scattering signals from 90 degree
27 scattering of 20, 40, 50, 60, 80, 100, and 200 nm gold nanoparticles using a green laser and standard
28 quartz cuvette were compared to the scattering signals from a green LED light source with an
29 oblate spheroid sample chamber and to Mie theory by fitting the data to a logistic curve. The
30 change in signal from 60 nm to 120 nm decreased in the order of Mie Theory > Optical Caustic
31 scattering > standard laser 90 degree scattering. These results suggested that conjugating 60 nm
32 gold nanoparticles with Dengue Protein E and using an optical caustic system to detect plasmonic
33 light scattering would result in a sensitive test for detecting human antibodies against Dengue
34 Protein E in serum. To explore this possibility, we studied the light scattering response of protein
35 E conjugated gold nanoparticles exposed to different concentrations of anti-protein E antibody,
36 and posteriorly via a feasibility study consisting of 10 human serum samples using a modified dot
37 blot protocol and a handheld optical caustic-based sensor device. The overall agreement between
38 the benchtop light scattering and dot blot results and the handheld optical caustic sensor suggest
39 that the new sensor concept shows promise to detect gold nanoparticle aggregation caused by the
40 presence of the antibody using a homogeneous assay. Further testing and protocol optimization is
41 needed in order to draw conclusions on the positive predictive and negative predictive values for
42 this new testing system.

43

44 Keywords: Arbovirus, Dengue, Nanoparticle, Optical Caustic, Protein E

45

46 **Background**

47 The development of a rapid and accurate means for identifying the cause of a systemic infection
48 has been a subject of intense interest due to the need for proper course of treatment in order to
49 improve patient outcomes. Also, there is a growing need for accurate diagnoses due to the toll in
50 human and economic terms caused by endemic diseases transmitted by mosquitoes in tropical
51 regions. Of particular focus in developing countries in the tropical region, is the ability to ascertain
52 whether a patient has contracted Dengue Fever and specifically which serotype (DEN-1, 2, 3, 4)
53 is the probable cause of the illness. While symptomatic diagnostics play an important role in all
54 febrile disease management, some patients are asymptomatic or have mild symptoms, and
55 diagnosis of these patients can be critical because Dengue Fever serotypes are believed to be
56 directly linked to severe courses of infection such as Dengue Shock syndrome (DSS) and Dengue
57 Hemorrhagic Fever (DHF), making early serotype identification a potentially valuable tool.
58 Moreover, confirmation of whether the patient has had a prior serotype infection, which has also
59 been linked to DSS and DHF, can also help to determine the course of treatment and further steps
60 to prevent an outbreak of Dengue [8-11].

61 In order to meet the need for a rapid diagnostic that can be implemented in the field and closely
62 based on patient exposure and/or immune response at an early stage of patient reported symptoms,
63 a hybrid approach that combines gold nanoparticle conjugates (similar to what is used in low-cost
64 paper diagnostics based on lateral flow immunoassay technology) with a high level of sensitivity
65 in conjunction with a portable sensor for detecting a positive response at low antigen levels is the
66 subject of this feasibility study. In order to establish a relatively low cost diagnostic tool, the
67 hybrid technology described in this paper builds upon the employment of an optical caustic light
68 scattering technology that employs no lenses and does not need filters [1]. Moreover, the use of
69 battery powered LEDs and the deployment of a smartphone to analyze the scattered light are also

70 helpful in reducing cost as well as in improving access to the device for low and middle income
71 countries.

72 To commence a process of verifying the capabilities of the new hybrid technology platform in a
73 simulated low resource setting, our approach was to first determine if an existing Dengue
74 molecular reagent used for gold nanoparticle conjugation in paper assays could detect Dengue
75 antibodies with human patient samples by employing this new hybrid technology platform. For
76 the first part of this study, we analyzed the 90 degree light scattering response of conjugated gold
77 nanoparticles to different concentrations of anti-Protein E antibody to determine key parameters
78 such as: (1) size of gold nanoparticle that should be used; and (2) stability of the gold nanoparticle
79 conjugates when subjected to transportation and varying temperature conditions. For the second
80 part of the study, a direct approach with clinically relevant samples was used since it is a faster
81 way to determine other important parameters such as: (1) whether very small amounts of human
82 serum samples can yield reasonable signals; (2) determine the need for additional dilution or
83 blocking steps when working with human serum; and (3) whether room or body temperature and
84 incubation time generate differences in measurement. Thus, the overall objective of this feasibility
85 study is solely to gain experience in practical aspects of developing a rapid and hybrid quantitative
86 assay for determining Dengue infection by monitoring patient antibody response while simulating
87 a low resource setting in order to expand testing in a variety of locales and with a wider variation
88 in infrastructure than is normally the case in high income country clinics and hospitals.

89

90 **Materials and Methods**

91 ***Gold Nanoparticle Light Scattering Calibration***

92 For calibration purposes, unconjugated gold nanoparticles of 20, 40, 50, 60, 80, 100, and 200 nm
93 (Ted Pella Inc., Reading, CA) were diluted 1:10 in distilled deionized water and analyzed for light
94 scattering and extinction using three separate detection methods. Each gold particle size sample
95 contained the same overall molar concentration of gold.

96 ***Gold Nanoparticle Conjugation***

97 In a 1.5 ml Eppendorf tube, an aliquot of 1 ml containing 2.6×10^{10} particles/ml of 60 nm gold
98 colloids (Ted Pella Inc, Redding, CA) was combined with 100 microliters of freshly prepared pH
99 = 8.5 borate buffer prior to the addition of 50 microliters of 0.85 mg/ml Protein E Dengue
100 Envelope-2 32 kDA (MCR-054, Reagent Proteins, Pfenex Inc., San Diego, CA). A frozen cold
101 pack was placed on the tube and the mixture was gently rocked using an orbital table for 30
102 minutes. This was followed by the addition of 2.5 microliters of 10% Tween 20 and rocking on
103 the orbital table for 5 more minutes.

104 One or three centrifugation steps were then conducted in order to reduce the concentration of
105 unbound Protein E form the suspension. A Beckman Coulter Microfuge 18 (Beckman Coulter,
106 Brea, CA) was placed in a 4°C environmental room in order to minimize aggregation of gold
107 nanoparticles and ensure resuspension after centrifugation. The first centrifugation was for 30
108 minutes at 3500g. Immediately after centrifugation, as much of the supernatant as possible was
109 carefully removed from the pellet using a 200 microliter micropipette, while not disturbing the
110 pellet. Once this was accomplished, 1 ml of pH = 8.5 borate buffer was added to re-suspend the
111 pellet. An aliquot of 2.5 microliters of 10% Tween 20 was then added to the suspension and the
112 mixture was gently rocked for 5 minutes. Afterwards, the suspension was centrifuged again for
113 15 minutes at 3500g. The same procedure was used following the second centrifugation as
114 described for the first centrifugation step. For the 3rd centrifugation, the time was shortened to 10

115 minutes. After the third and final centrifugation, the pellet was re-suspended in 0.5 ml of a 0.2
116 mg/ml solution of Bovine Serum Albumin (BSA) in DI water to block the remaining unreacted
117 sites on the gold nanoparticles. The particles were then incubated on the orbital table for an
118 additional 5 minutes. This was followed by the addition of 0.5 ml of DI water and 0.5% sodium
119 azide.

120 ***Detection of anti-Protein E antibody in vitro***

121 To 100 μ l of conjugated gold nanoparticles, 900 μ l of PBS were added. Posteriorly, 10 μ l of
122 different concentrations of anti-Protein E antibody were added prior to measuring 90-degree light
123 scattering using the oval plastic chamber and the handheld optical caustic sensor which used a
124 Nokia 920 smartphone and Lumia software for imaging. Pictures of the oval chamber were taking
125 using different times of exposure (0.1 sec or 1 sec) and by reducing overall brightness to the lowest
126 level in the Lumia camera app. The images were analyzed measuring the raw intensity using
127 ImageJ using the green or red channel, depending upon the level of saturation of the green channel,
128 and by focusing in the zone of the sample chamber where scattering by the gold nanoparticles
129 provides pixels with brightness above the typical PBS solution pixel values of 0-5 (out of a
130 maximum range of 255).

131 ***Dot Blot using conjugated Gold nanoparticles***

132 Standard dot blot paper (Bio Rad Laboratories, Hercules, CA) was cut into rectangular or
133 hexagonal shapes in order to fit into 12 well Corning Costar Tissue Culture Plates (Ted Pella Inc.,
134 Reading, CA). After punching a hole in the center of the paper with a sterile pin, 3 microliters of
135 1:100 PBS diluted human serum was placed over the area around the pin hole and allowed to dry
136 for 5 minutes at 37 °C. Then, the paper was cooled to 4 °C and allowed to incubate for 15 minutes.
137 Following incubation, an aliquot of 1 ml of a 3% skim milk in PBS blocking solution was added

138 to the chamber and mixed for 15 minutes at room temperature. After incubating in the blocking
139 solution for 30 minutes at 37 °C, an aliquot of 500 microliters of a 1:10 diluted suspension of 60
140 nm Protein E conjugated gold nanoparticle was added to the paper. Incubation with the gold
141 nanoparticle conjugate was conducted for 1 hour at 37 °C. After the final incubation, the paper
142 was rinsed 3 times in PBS – Tween 20 buffer and allowed to dry.

143 ***Testing of Human Serum Samples***

144 All human serum samples were obtained voluntarily from Hemolab S.A. and the Lab of
145 Arbovirology of the Universidad Autonoma de Yucatán collected for previous studies. Two 6 ml
146 bottles of conjugated gold nanoparticle reagent GNP-60-E were created according to the protocol
147 described above except that while one GNP reagent (GNP-60-E-3) was centrifuged 3 times to
148 remove unbound Protein E, a second reagent (GNP-60-E-1) was centrifuged only once. Both
149 reagents were stored for 16 hours at 4 °C then transported at room temperature for 19 hours, until
150 refrigerated at 4 °C at the Universidad Autónoma de Yucatán (UADY). Both GNP-60-E reagents
151 arrived un-aggregated at UADY based on both Nanodrop spectrometer (Bio Rad Laboratory,
152 Hercules, CA) visible spectra taken at the Universidad Autónoma del Yucatán (UADY) before
153 using the reagents and by visual observation of the gold nanoparticle suspension.

154 For each test, in a 1.5 ml Eppendorf tube, 900 µl of PBS were combined with 100 µl of the gold
155 nanoparticle conjugate followed by the addition of 5 or 10 microliters of the human serum samples
156 or a negative control of PBS. For the testing at 37 °C, GNP-60-E-3 was used and 10 microliters of
157 undiluted human serum was added. Incubation was performed for 30 minutes at 37 °C without
158 agitation. Afterwards, each test sample was placed in an oblate spheroid chamber and capped,
159 followed by imaging with the smartphone sensor. For the first trial at 22 °C, GNP-60-E-3 was used
160 and 5 microliters of undiluted human serum was added. Incubation was performed for 15 minutes

161 at 22 °C without agitation. Afterwards, each test sample was placed in an oblate spheroid chamber
162 and capped, followed by imaging. For the second trial at 22 °C, GNP-60-E-1 was used and 2
163 microliters of 1:10 diluted human serum was added. Incubation was performed for 15 minutes at
164 22 °C without agitation. Afterwards, each test sample was placed in an oblate spheroid chamber
165 and capped, followed by imaging.

166 ***Light Scattering Measurement Systems***

167 For 90-degree laser light benchtop scattering measurements, an Ocean Optics Fiber Optic
168 Spectrometer (Ocean Optics, Dunedin, FL) was used with a USB4000 spectrometer and
169 SpectraSuite Software for control and data acquisition. A quartz cuvette of 1 cm path length with
170 all four windows clear for measurement enables 90-degree placement of an InPhotonics 532 nm
171 laser, with an Ocean Optics controller from the fiber optic collector, to measure counts of scattered
172 light. Readings of 1 second integration time with 5 spectra averaging was used.

173 ***3D Printed Oblate Spheroid Chamber***

174 Autodesk Fusion 360 software was used to generate the 3D oblate spheroid sample chamber used
175 in the handheld optical caustic sensor. In order to place the sample chamber in the LED
176 illumination chamber and easily remove it after imaging, a solid rectangular peg was added to the
177 center of the base. The opening of the sample chamber was sized and designed with a small ridge
178 in order to accommodate lids cut from 200 microliter PCR tubes. Fabrication of the sample
179 chambers were done in batches of 12 by transmitting the drawing to a 3D printing company
180 (iMaterialise, Leuven, Belgium). 3D printing is conducted using stereolithography with a
181 transparent resin and the finished product is between water clear and translucent, in terms of
182 visibility to the naked eye.

183 ***Handheld Smartphone Optical Caustic Light Scattering Sensor***

184 A previously described handheld smartphone-enabled optical caustic light scattering sensor was
185 used to capture images of samples in an oblate spheroid chamber [1]. A 532 nm green Photodiode
186 (Industrial Fiber Optics, Tempe, AZ) illuminated the sample chamber at a 90° angle from a Nokia
187 Lumia 920 (Nokia, Espoo, Finland) smartphone camera lens. Images were collected at 0.5 second
188 exposure using the Lumia camera app. At this exposure level, and with the intensity of light used,
189 the green channel of the RGB images saturate. However, excess light due to scattering can be
190 imaged in the center of the sample chamber by splitting the color channels using ImageJ (NIH,
191 Bethesda, MD). ImageJ software was used to collect the intensity of the red, green, and blue
192 channels for each image. Integrated density measurements from ImageJ was collected for a
193 constant image area and used to quantify the amount of scattering observed for gold nanoparticles
194 in water, conjugated gold nanoparticles with a serum sample, or a Phosphate Buffered Saline
195 (PBS) control.

196 ***Digital Color Optical Caustic Light Scattering Sensor***

197 In lieu of a smartphone to collect images and in order to corroborate the gold nanoparticle
198 scattering vs. size calibration with the optical caustic sample chamber, a Digital Color Sensor
199 S9706 (Hamamatsu Photonics, Hamamatsu, JP) collected light from the oblate spheroid sample
200 chamber at a 90° angle and a distance of 10 mm from the center of the chamber. Due to the
201 proximity of the sensor to the sample chamber, a 3-D printed tubular mask with an opening of 7
202 mm in diameter was used to block the incident light. A 3-D printed chamber with interior angled
203 walls was also fabricated and used to minimize light reflection. The digital color sensor was
204 connected to an Arduino Uno computer and the manufacturer's recommended algorithm was
205 deployed to acquire data at different integration times. Data for the gold nanoparticles in water
206 was acquired using between 0.1 - 30 seconds integration time. Since a lower intensity of LED

207 light was used than with the smartphone system, data for 20, 40, 50, 60, 80, 100, and 200 nm was
208 collected for the green channel of the sensor. The most accurate data to compare scattering using
209 the digital color sensor in this system was the highest integration time of 30 seconds, which was
210 then used to compare with the smartphone light scattering results.

211

212 **Results and Discussion**

213 Before conjugation of Protein E to gold nanoparticles, the choice of gold nanoparticle size was
214 deemed to be a key variable that needed to be determined. Based on the well understood properties
215 of gold nanoparticles to light scattering via plasmon resonance [6] near the maximum for spheres
216 of 520-540 nm, a calibration was conducted with a laser light scattering fiber optic spectrometer,
217 the optical caustic sensor, and calculations based on Mie Theory [6]. Figure 1 illustrates two key
218 points. First, that the laser light scattering system which is based on 90 degree scattering is
219 sensitive to small changes in particles size at a narrow range of between 30-70 nm diameter
220 particles. Mie Theory calculations illustrate that the total scattering for gold nanoparticles
221 increases more gradually with size, since this calculation takes into account all angles of scattering.
222 The Optical Caustic sample chamber is seen in Figure 1 to fall between the two groups of data,
223 using both a camera and a digital color sensor to collect data. It was also found that the red channel
224 of the smartphone RGB image was most useful based on the LED intensity and shutter speed
225 setting since smartphone sensor saturation “bleeds” signal to the red and blue channels when there
226 is an excess of green in the image. The digital color sensor corroborates that interpretation, as
227 shown in Figure 1.

228

229 **Figure 1.** Comparison of gold nanoparticle scattering with green light data for a laser and fiber
230 optic spectrometer, LED/optical caustic smartphone, and LED/optical caustic digital color sensor.
231 Discrete calculations of the total scattering at 532 nm using Mie theory is also shown. Data and
232 calculations are normalized to the maximum value for gold nanoparticles of 200 nm and fitted to
233 a logistic curve. Horizontal dashed lines illustrate the signal difference for 60 and 120 nm diameter
234 gold nanoparticles.

235

236 The overall interpretation of the calibration data is that using 60 nm gold particles is very practical
237 for the intended application. The reason for this is that there is a dramatic (approximately 340%)
238 increase in signal predicted when two 60 nm gold particles aggregate upon antibody-antigen
239 binding, basically the change in relative signal from 60 nm to 120 nm gold particle size.

240 After establishing that 60 nm gold particles would be a useful size, it is also important to note that
241 conjugated gold nanoparticles are sensitive optically to any surface change, including binding of
242 antibodies or antigens to their surfaces and the additional binding of proteins to their surfaces or
243 aggregation of gold nanoparticles. To establish the response of the system in terms of 90-degree
244 light scattering near the plasmon resonant peak, different amounts of anti-Protein E antibody were
245 added to a diluted solution of conjugated gold nanoparticles. The first parameter to determine was
246 the zone for no scattering in the chamber, and in this case PBS without gold nanoparticles was
247 used. Images taken with 1 sec of exposure and analyzed using the red channel since the green
248 channel was already saturated with green light (Figure 2B) shows that when using PBS, the amount
249 of light detected from the center of the sample chamber is very low since no scattering nor
250 reflection is expected in this zone of the sample chamber. Other images using different exposure
251 times with the green channel did not provide a sufficiently good baseline dark zone, so the most

252 appropriate exposure time for imaging for the handheld optical caustic smartphone was determined
253 to be a 1 sec exposure in the center zone of the images' red channel.

254

255 **Figure 2. Light scattered using PBS or gold nanoparticles in the oval chamber.** A) Light
256 scattering intensity of PBS measured with the green channel of a picture taken with 0.1 sec of
257 exposure time. B) Light scattering intensity of PBS measured with the red channel of a picture
258 taken with 1 sec of exposure time. C) Light scattering intensity of 60 nm gold nanoparticles
259 measured with the red channel of a picture taken with 1 sec of exposure time.

260 The table in the figure represent the gray values for the area inside the circle for each sample.

261

262 Next, images were taken for an aqueous suspension of 60 nm gold nanoparticles using the same
263 imaging settings as for PBS. Figure 2C shows that the region given as a dark area when imaging
264 PBS, now contains brightness due to gold nanoparticle light scattering. The integrated difference
265 for these two measurements is on the order of 100x, which clearly provides a high range for
266 detecting small changes in gold nanoparticle scattering. It is important to note that this signal is
267 based on only ~1.8 billion gold nanoparticles in 0.7 ml of suspension, which suggests that detection
268 to a sensitivity of 50 pg/ml of antibody or antigen should be possible since it could represent a 1%
269 difference in nanoparticle scattering signal.

270 Finally, in order to quickly explore the range of signal change possible for a commercially
271 available Protein E antigen with the handheld optical caustic sensor, the light scattering intensity
272 for a gold nanoparticle suspension and gold nanoparticles containing Protein E in the presence of
273 10 μ g/ml of anti-Protein E antibody in PBS. Table 1 gives the gray value differences for the
274 controls and the antibody test.

275 **Table 1. Average gray values as a light scattering measurement for samples.** Mean gray values
276 for samples of PBS, gold nanoparticles, and gold nanoparticles with 10 µg/ml of anti-protein E
277 antibody, in the oval chamber.

Sample	PBS	Gold nanoparticles	Gold nanoparticles with 10 µg/ml of anti-protein E antibody
Area (a.u.)	49628	49628	49628
Mean gray value (a.u.)	1.181 ± 0.737	146.214 ± 10.233	159.800 ± 7.658

278

279

280 The initial challenge lay in interpreting patient results without an extensive study of the antigen
281 protein structure nor its immunogenic properties when presented on gold nanoparticle surfaces.
282 This makes discerning the performance of the tests with respect to patient Dengue status
283 characterization challenging. The challenge is somewhat reduced by using a dot blot test with the
284 same patient samples and gold conjugate reagents as an orthogonal test. Table 2 provides
285 information on the 10 patient serum samples donated by the Arbovirus laboratory of UADY for
286 this study. These samples represent a spectrum of patients including Dengue negative, Dengue
287 serotype 2 positive with a first time (primary) infection and 2nd time (secondary) infection, patients
288 convalescing from a Dengue serotype 2 infection, and patients with Dengue serotypes 1 and 3,
289 respectively. Patients with early stage and primary dengue infection should present IgM against
290 dengue antigens after a few days of infection and the IgM levels should decrease after 90 days [3-
291 5, 8-11]. Patients with a secondary infection should mostly present IgG antibodies [5, 8-11]. The
292 antigen Protein E used as the reagent conjugated to the gold nanoparticles is a recombinant protein
293 with selectivity towards Dengue Serotype 2 antibodies and is described by the manufacturer as
294 being most sensitive to IgM levels. However, it is known that there can be cross-reactivity to other
295 dengue serotype antibodies as well as from patients who have experienced other arbovirus
296 infections from the group known as flaviviruses such as West Nile, St. Louis Encephalitis, Zika

297 Virus, and Chikungunya [4]. These considerations suggest that there should be some variation in
298 test results, but the variations may be difficult to discern without a more comprehensive series of
299 human serum controls.

300

301 **Table 2. Description of human serum samples.** Human serum samples used in the feasibility
302 study with descriptive information on Dengue status.

Patient	Dengue Status	Description of Sample	Primary or Secondary Infection	Stage of Disease
1	Negative	Asymptomatic, healthy individual, PCR-IgM-IgG negative for Dengue Virus	N.A.	N.A.
2	Negative	Asymptomatic, healthy individual, PCR-IgM-IgG negative for Dengue Virus	N.A.	N.A.
3*	DENV-2	PCR positive for DENV-2, IgM positive for DENV-2, IgG negative for DENV-2	Primary	Initial stage
4*	DENV-2	PCR positive for DENV-2, IgM positive for DENV-2, IgG negative for DENV-2	Primary	Initial stage
5	DENV-2	Seropositive for DENV-2, IgM negative for DENV-2, IgG elevated for DENV-2, day 4	Secondary	Initial stage
6	DENV-2	Seropositive for DENV-2, IgM negative for DENV-2, IgG elevated for DENV-2, day 4	Secondary	Initial stage
7	DENV-3	PCR positive for DENV-3	Unknown	Initial stage
8	DENV-1	PCR positive for DENV-1	Unknown	Initial stage
9**	DENV-2	Volunteer donated sample, seropositive for DENV-2, IgM positive for DENV-2	Unknown	Convalescing > 120 days
10**	DENV-2	Volunteer donated sample, seropositive for DENV-2, IgM positive for DENV-2	Unknown	Convalescing > 120 days

303 *Patients positive for dengue with negative IgG test.

304 **Patients volunteered for testing were positive with DENV-2 during the epidemic in 2015 and
305 donated samples 4 months after initial diagnoses.

306

307

308 Before commencing patient testing, the 60 nm gold conjugates were inspected and the UV/VIS
309 spectra were recorded for the two batches of particle conjugates (Figure 3). Both visual and
310 spectral information verified that the gold conjugates were stable and ready to use at UADY.

311

312 **Figure 3. Nanodrop spectrometer UV/VIS spectra.** The absorbance in the UV is due to the
313 BSA blocking solution. The absorbance maxima at a wavelength of 540 nm is consistent with the
314 expected plasmon resonant peak for conjugated gold nanoparticles of 60 nm diameter.

315
316 Table 3 summarizes the expected dot blot score based on the protein E gold conjugate reagent
317 (GNP-60-E-3) used, assuming some level of cross-reactivity with other Dengue serotypes and a
318 50% probability of measuring antibodies reactive to Protein E after 120 days of convalescence.
319 The individual blot samples and the scores of the dot blot are shown in Figure 4 and in Table 3.

320
321 **Figure 4. Image showing visual scoring of dot blots.** Each blot was done in separate paper and
322 reaction chambers in order to limit solution volume for gold conjugation and prevent cross
323 contamination among the human serum samples and PBS negative control.

324
325 **Table 3. Comparison of results of the human serum samples between diagnostic methods.**
326 Comparison of Dot Blot with Expected Result due to Dengue Status reported by the clinical
327 laboratory. The Protein E used while specific for DENV-2, has sensitivity for IgM detection and
328 can have cross-reactivity with other serotypes.

Patient	Expected Dengue Result Based on Dengue Serotype and Some Cross-Reactivity (assuming high sensitivity to IgM)	Dot Blot Score (+ or -)	Agreement
1	-	+	NO
2	-	+	NO
3	+	+	YES
4	+	+	YES
5	-	-	YES
6	-	-	YES
7	-	-	YES
8	+	+	YES
9	+	+	YES
10	-	-	YES

329

330 Overall, the agreement is very good. However, the two dengue negative patients appear to give
331 positive dot blot results. It is not clear why this is the case, but perhaps a current or prior flavivirus
332 infection is being detected by the gold conjugate reagent. Additionally, the sample with PBS added
333 and no human serum was correctly identified as a negative control in the dot blot experiment. It
334 is also important to note that a dot blot test (not shown) with a monoclonal antibody that reacts
335 with flavivirus group specific antigens (4G2, KPL) was found to be negative. The negative result
336 suggests that epitopes of the protein envelope needed for the monoclonal antibody to bind to the
337 GNP-60-E-3 were blocked due to the immobilization of Protein E to the gold nanoparticles. This
338 is a potentially useful observation for further gold conjugate development, namely if a
339 methodology for Protein E binding to gold based on covalent attachment rather than his-tag is
340 used.

341 A summary of the three sets of tests with human serum samples and an overall score is given in
342 Table 4 while a quantitative comparison of the dot blot is shown in Figure 5. The overall score
343 given in Table 3 is based on assessing the differences among the three tests using gold
344 nanoparticles made with either 3 or 1 centrifugation step(s) and at different times and temperatures.
345 Based on the results in Table 3, it appears that the results with GNP-60-E-1 at 22 C for 15 minutes
346 seem to be most closely related to the characterization based on the dengue patient status
347 information.

348

349 **Figure 5. Comparison of Dot Blot and Optical Caustic Smartphone Sensor.** Data were
350 recorded at the same sample incubation temperature of 37 C.

351

352

353 **Table 4. Qualitative summary of Optical Caustic Scattering Smartphone Sensor data.**

Patient	GNP-60-E-3 37 C for 30 min	GNP-60-E-3 22 C for 15 min Trial 1	GNP-60-E-1 22C for 15 min Trial 2	Overall Score (+ or -)
1	weak positive	<i>positive</i>	negative	-
2	positive	<i>negative</i>	positive	+
3	positive	<i>positive</i>	positive	+
4	positive	<i>positive</i>	weak positive	+
5	positive	<i>positive</i>	positive	+
6	positive	<i>negative</i>	positive	+
7	negative	<i>weak positive</i>	negative	-
8	positive	<i>positive</i>	negative	-
9	positive	<i>weak positive</i>	positive	+
10	very weak positive	<i>positive</i>	positive	+
PBS Control	negative	<i>negative</i>	negative	NEGATIVE CONTROL
PBS Control	negative	<i>negative</i>	negative	NEGATIVE CONTROL

354

355

356 In Figure 5, there are two overall features to note. First it appears that the smartphone signal
 357 saturates at low “signals” from the dot blot experiments. This seems reasonable given the high
 358 signal change described in Figure 1 and 2 for aggregates consisting of 60 nm gold particles. The
 359 second feature is that the negative control and patient sample 10 are both low for the dot blot and
 360 the optical caustic sensor, but there is disagreement between patient samples 5 and 6 between the
 361 two detection methods. This may be due to the higher sensitivity of the optical caustic sensor as
 362 compared to the dot blot which used gold nanoparticles at a higher level of dilution. Dot blots are
 363 also considered to be lower in sensitivity due to diffusion and orientation effects when binding to
 364 a fixed surface.

365 Another observation is that patient sample 7 yielded a very weak signal and patient sample 10 is
366 negative based on the dot blot tests, yet the optical caustic sensor data show strong signals. This
367 again may be due to higher sensitivity of the optical caustic system and cross reactivity of the
368 Dengue Serotype 2 recombinant Protein E with other Dengue serotypes. As noted in the results
369 for GNP-60-E-1 at 22 C and 15 minutes seen in Table 4, it appears that this cross-reactivity may
370 be diminished by using a higher dilution of human serum, lower temperature, and allowing some
371 unbound antigen in the gold nanoparticle conjugation suspension.

372

373 **Conclusions**

374 A feasibility study of a hybrid gold nanoparticle with an optical caustic sensor system indicates
375 that the technology is sensitive to the detection of serum antibodies against dengue fever. The use
376 of similar size gold nanoparticles (60 nm) to what is often used in paper lateral flow rapid tests is
377 justified based on calibration data and human patient sample testing. The gold nanoparticle
378 conjugates are stable to transportation and temperature fluctuations and appear to be un-aggregated
379 and active after several days of conjugation. Also, all negative controls for the dot blot and optical
380 caustic sensors were correctly measured as negative.

381 Dot blot tests were found to be useful to verify the reactivity of the gold nanoparticle conjugates
382 to patient serum antibodies and may also help identify epitope presentation differences when
383 applying monoclonal antibodies to the dot blot paper directly. It appears that human serum should
384 be diluted and that testing can be done at around 22 °C within 15 minutes using the hybrid gold
385 nanoparticle conjugate reagent and optical caustic sensor. A more thorough investigation of well
386 characterized human serum samples is still needed in order to optimize the test conditions and

387 buffer components and generate positive predictive and negative predictive values that reflect the
388 capabilities of the diagnostic platform.

389

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